# Challenges in transcatheter aortic valve implantation 

Stefan Toggweiler ${ }^{a, b}$, John G. Webb ${ }^{a}$

a St. Paul's Hospital, University of British Columbia, Vancouver, Canada<br>Luzerner Kantonsspital, Lucerne, Switzerland


#### Abstract

Summary Although safety and efficacy of TAVI was improved with next-generation equipment, experience, and careful patient selection, some worrisome complications associated with the procedure remain. Current hot topics in transcatheter aortic valve implantation include patient selection, valve sizing, paravalvular regurgitation, cerebrovascular accidents, vascular complications and need for a permanent pacemaker. In this article we review the pathophysiology, avoidance and treatment options for these complications.


Key words: aortic valve; transcatheter aortic valve implantation; transcatheter aortic valve replacement; complications; vascular; cerebrovascular; stroke; valve sizing

## Introduction

Transcatheter aortic valve replacement (TAVI) has emerged as the current therapy of choice in patients with severe aortic valve stenosis who are not candidates for open-heart surgery $[1-3]$, and as an alternative to high risk surgery in patients who are operable [4]. Although safety and efficacy of TAVI has improved with next-generation equipment, experience and careful patient selection, some worrisome complications associated with the procedure remain. In this paper we review some of the challenges the operator faces when performing TAVI, including patient selection, valve sizing, cerebrovascular events, vascular complications and need for a permanent pacemaker. A review article by Ferrari and von Segesser discussing different valve and access routes has been previously published in this journal [5].

## Patient selection

Studies with long-term follow-up have shown that with current patient selection median survival after TAVI is $\sim 3$ years $[3,6]$. Therefore, TAVI should probably not be performed in the presence of relevant comorbidities that limit life-expectancy to less than 2-3 years. Also, TAVI should result in significantly improved quality of life. Patients
should be discussed and selected by a multidisciplinary heart team including cardiologists and surgeons [7]. There are subgroups of patients that may be excellent candidates for TAVI (porcelain aorta, previous coronary artery bypass grafting).

## Inoperable patients

The PARTNER trial (cohort B) randomised inoperable patients to medical therapy or transfemoral TAVI [1]. The Society of Thoracic Surgeons' (STS-Score) predicted rate of periprocedural mortality was $11 \%$, the actual 30 -day mortality was $5.0 \%$ with TAVI and $2.8 \%$ with medical treatment. At 1 year mortality was $30.7 \%$ with TAVI compared with $50.7 \%$ with medical treatment, representing an impressive absolute reduction of $20 \%$. However, the high mortality rate of $30.7 \%$ in patients treated with transfemoral TAVI indicates that many patients died from their comorbidities. Subgroup analyses have shown that patients with a very high risk (STS score $>15 \%$ ) did not derive benefit from TAVI. Hence in the presence of multiple (non-cardiac) comorbidities TAVI may be less effective since some patients are likely to die from other, non-cardiac causes ("futility").

## High-risk patients

In cohort A of the PARTNER trial, patients with a mean STS score of $11.8 \%$ were randomised to TAVI and surgical AVR. Actual 30 days' mortality was $3.4 \%$ with TAVI and $6.5 \%$ with SAVR $(p=0.07)$ [4]. Mortality 1 year after randomisation was $24.2 \%$ with TAVI and $26.8 \%$ with surgical AVR. TAVI was associated with a lower rate of bleeding, a shorter hospital stay and more vascular complications. There was a non-significant trend to more strokes with TAVI, but the combined risk of death or major stroke was nonsignificantly lower with TAVI.

## Intermediate- and low-risk patients

Large studies comparing TAVI to surgical AVR in intermediate risk patients are currently under way (Surgical Replacement and Transcatheter Aortic Valve Implantation (SURTAVI) and PARTNER II). As a result of improve-
ments in TAVI technology, experience and outcome in registries, it appears reasonable to offer TAVI to patients who would otherwise be considered intermediate to low risk where there is a consensus of the heart team that they are at significantly increased risk of morbidity or mortality due to special circumstances [7]. There is evidence that improved outcomes can be expected in lower surgical risk patients undergoing TAVI [8, 9].

## Valve siting / paravalvular regurgitation



Figure 1
Annulus sizing using TEE and CT angiography. TEE measured an annulus of 2.1 cm suggesting a 23 mm Edwards Sapien or a 26 mm Medtronic CoreValve (A). CT angiography measured an area of 481 mm 2 (C) and a mean diameter of 24 mm (B) suggesting a 26 mm Edwards Sapien or a 29 mm Medtronic CoreValve valve with $\sim 10 \%$ oversizing. A 26 mm Edwards Sapien valve was implanted with trace paravalvular leak (D).


## Figure 2

Treatment of paravalvular regurgitation by implantation of a second transcatheter heart valve.
In patient, the TEE measured an annulus of 22 mm . A 26 mm Edwards Sapien XT valve was implanted (A). A low implantation resulted in severe paravalvular aortic regurgitation (B, C). A second 26 mm valve was subsequently implanted in a higher position, thus extending the annular seal (D) resulting in a mild paravalvular leak (E, F).

## Annular sizing

Unlike in open heart surgery, where the aortic annulus can be directly inspected and sized intraoperatively, TAVI operators depend on external, indirect measurements of the annulus. Correct sizing of the annulus and choice of prosthesis is of the utmost importance if paravalvular leakage, device embolisation and annular rupture are to be avoided. Traditionally the annulus has been measured with 2-dimensional echocardiography, with TTE in the parasternal long-axis view or with TEE in the $\sim 130^{\circ}$ view. Recent research has shown that the annulus is an oval structure where the long axis is on average $5-6 \mathrm{~mm}$ (approx. $20 \%$ ) longer than the short axis [10, 11]. In patients with an oval-shaped annulus, one-dimensional diameter measurements may not be accurate and computed tomography (CT) may therefore be superior since it allows reconstruction and measurement of the annulus in its true plane. Threedimensional TEE may offer the same advantages but this technique needs further investigation [12]. Several studies have shown that CT-measured mean annular diameters are usually $1-2 \mathrm{~mm}$ larger than TEE-measured one-dimensional diameters, thus resulting in recommendation of a larger prosthesis size in up to $40 \%$ of patients [10, 11, 13] (fig. 1). So far there is no evidence that this practice leads to increased frequency of annular rupture, but a recent study has shown that the degree of paravalvular regurgitation was less if the prosthesis was chosen on the basis of CT instead of echocardiographic measures [14]. Currently CT is on its way to becoming the gold standard for annulus measurement and choice of valve prosthesis size. Mean annular diameter, perimeter, and annular area have all been proposed to serve as the main parameter for prosthesis selection. During the cardiac cycle the generally elliptic aortic annulus assumes a more round shape in systole, thus increasing cross-sectional area. Circumference remains relatively constant during the cardiac cycle and may therefore be the better parameter to measure [15]. After implantation of a balloon-expandable valve (to a lesser degree also after implantation of a self-expanding valve), the area increases when an oval annulus becomes more circular, but there are no major changes to the circumference. Implanting a valve based on annular area may therefore lead to undersizing in the case of a very oval annulus. However, there is some evidence that area measurements may be more reproducible than circumference measurements with a higher inter-observer and a higher intra-observer correlation [11, 16]. Overall, it is currently unclear which of the measurements will prevail and will become the new gold standard for annular sizing.

## Paravalvular regurgitation

Paravalvular regurgitation (PAR) is the result of undersizing and/or malpositioning of valves. Several studies have demonstrated an association between the degree of calcification of the native aortic valve cusps and the severity of PAR [17-19]. Grading of PAR has been done with echocardiography, angiography, and simultaneous pressure measurements of the aorta and the left ventricle [20]. In the PARTNER trial, postprocedural moderate or severe PAR was reported in 11.8 and $12.2 \%$ of patients after TAVI [1, 4]. At 1 year these rates were $7.0 \%$ after TAVI vs. $1.9 \%$
after surgical AVR. At 2 years, the respective rates were $6.9 \%$ and $0.9 \%$ [6]. In other publications the proportion of patients with postprocedural moderate or severe PAR ranged from 5.2-21\% [21-26]. Several studies have consistently shown that moderate or severe paravalvular regurgitation is associated with increased mortality after both surgical AVR [27] and after TAVI with odds/hazard ratios ranging from 2.4-3.8 [20, 22, 28]. In the PARTNER trial, even mild paravalvular regurgitation was found to be significantly associated with increased mortality (hazard ratio of 2.11 for $\geq$ mild PAR compared to none or trace PAR) [6]. However, some questions about this finding remain. First of all, mild regurgitation of native valves is usually very well tolerated and it would be surprising if mild PAR affected clinical outcome during such a short follow-up period. One explanation for the excess mortality may be that these patients had more calcified valves, complex procedures and comorbidities, and that mild PAR was a bystander rather than the main culprit for mortality. In the PARTNER patients mortality between 2 and 3 years was higher in patients with mild PAR than in patients with moderate to severe PAR, a finding that is not intuitive [6]. Furthermore, severity of PAR is difficult to measure since multiple and eccentric jets may be present.

## Treatment of paravalvular regurgitation

If relevant PAR occurs, the next step is to assess whether or not the valve is deployed in the correct position. If the valve is in the correct position postdilation may reduce the degree of PAR. If the valve appears undersized after postdilation the options are more limited, although paravalvular leak closure may be considered an option. However, most of the published data relate to paravalvular leak closure with surgically implanted valves, and experience with transcatheter valves is limited [29]. With transcatheter heart valves the shape of the leak may be circumferential and more than one leak may be present, making paravalvular leak closure more difficult or even impossible. In the event of malpositioning of the first valve, a second valve can be implanted higher (if the initial implant is too low) or lower (the initial implant is too high) than the first valve (fig. 2 ). The goal is to extend the sealing fabric in such a way that the sealing fabric of both valves overlaps and that the second valve ensures sealing with the native valve annulus $[30,31]$. The same valve size is used for both valves.

## Stroke

## Clinical relevance of cerebrovascular accidents

Cerebrovascular accidents (CVA) have emerged as one of the most worrisome and most discussed complications in TAVI. In the PARTNER trial the rate of strokes at 30 days ( $4.6 \%$ vs. $2.4 \%$ ), 1 year ( $6.0 \%$ vs. $3.2 \%$ ) and 2 years ( $7.7 \%$ vs. $4.9 \%$ ) was not significantly higher after TAVI than after SAVR [4, 6, 32]. Predictors for CVAs were prior CVA, a smaller indexed aortic valve area, higher NYHA class, prior stroke, history of PCI, and absence of COPD [32]. It has been shown that some $50 \%$ of CVAs occur within the first 2 days after TAVI and are associated with a 3.5-5 fold increased mortality [22, 32, 33].

Periprocedural CVAs may result from embolisation of calcified microdebris during positioning and deployment of the valve, but also during passage of the aortic arch with the guidewire and the catheter, during balloon valvuloplasty or re-capture of a valve. Air embolism may be a concern, especially in patients undergoing transapical TAVI. Some of the next generation valves offer the possibility of recapturing and re-positioning in the event of initial valve malposition [34]. However, additional manipulation and replacement of valves, as well as postdilation, have been associated with higher stroke rates [35, 36]. Cerebrovascular accidents not infrequently occur during the first 1-2 days after the procedure. These postprocedural strokes may be due to the non-endothelialised and thrombogenic bioprosthesis itself, new-onset atrial fibrillation, late calcific embolism, or possibly late thrombosis or haemorrhage following earlier embolism [37, 38].
In larger recent studies, the rate of acute strokes ranged from 0.8 [39] to $6.7 \%$ [1, 4, 22-25, 40-44], but the rate of


Figure 3
Silent bilateral cerebrovascular emboli after transcatheter aortic valve implantation.
Such diffuse, bihemispheric ischaemic lesions can be detected by MRT in 68-77\% of patients after TAVI.


## Figure 4

Example of an embolic protection device.
The Embrella embolic deflector (A, Embrella Cardiovascular Inc, Wayne, PA) is introduced through the right radial artery to protect the brachiocephalic artery (BA), the left carotid artery (LCA) and the left subclavian artery (LSA) during the procedure.
silent cerebral ischaemia after TAVI was found to be much higher. Risk factors for cerebral embolisms are summarised in table 1.

## Magnetic resonance and Doppler ultrasound studies

To investigate silent cerebrovascular embolism, Kahlert et al. performed diffusion-weighted magnetic resonance tomographies (MRT) in patients undergoing TAVI $(\mathrm{n}=32)$ and open surgical aortic valve replacement $(\mathrm{n}=21)$ [45]. After a median of 3.4 days post procedure new foci were found in $84 \%$ of patients undergoing TAVI (fig. 3 ). There was no clinical stroke in the TAVI group (but one stroke in the SAVR group), and there was no difference between the balloon-expandable Sapien valve (Edwards Lifesciences Inc, Irvine, CA) and the self-expanding CoreValve (Medtronic Inc., Minneapolis, MN). At 3 months the majority $(80 \%)$ of the acute lesions had resolved. These findings were confirmed by other studies, showing that diffuse bihemispheric ischaemic lesions can be detected by MRT in 68-77\% of patients after TAVI [46-49]. No differences between the transfemoral and the transapical approach were found, although some have suggested that transapical TAVI may result in less trauma to the aortic valve and aortic arch, since less manipulation of catheters is needed [46, 50]. However, there is no evidence to support this. The incidence of clinically relevant strokes correlated with the number and size of lesions on MRT in some [49] but not all studies [47]. Therefore the clinical significance of these lesions remains unclear, although evidence from the surgical literature indicates that multiple, apparently silent, cerebral infarctions increase the risk of neurological dysfunction and cognitive decline [51].
Several studies used transcranial Doppler ultrasound (TCD) with the aim of quantifying the high-intensity transient (HITS) and microembolic signals (MES) during different stages of the procedure. In transapical balloon-expandable TAVI with the Edwards Sapien valve, most HITS and MES were counted during balloon valvuloplasty and valve delivery [52], but also during manipulation of the wire in the aortic arch [53, 54]. Severe calcification of the arch was identified as a predictor for HITS [54], but the number of HITS did not differ between transfemoral and transapical procedures [53,54]. One study showed an overall higher rate of HITS during TAVI with the self expanding CoreValve than the balloon-expandable Sapien valve, but with both valves most HITS occurred during valve deployment [53]. However, the number of HITS did not correlate with new lesions on cerebral CT. Furthermore, the high amount of HITS and new lesions on cerebral CT contrasts with the low rate of clinical cerebrovascular events.

## Embolic protection devices

Several strategies to reduce acute stroke rate have been suggested. These include not performing BAV, minimising the passage of guide wires and catheters across the aortic arch, and utilisation of embolic protection devices [32, 55-57]. Strategies to reduce the rate of late CVAs include oral anticoagulation in the event of new onset atrial fibrillation.
Different embolic protection devices are currently in use and under investigation [57-59]. These devices are introduced at the beginning of the procedure either through the right radial or the femoral artery and their aim is to protect the brachiocephalic and left carotid artery from embolic material (fig. 4 ). An ideal protection device would be minimally invasive, easy and rapid to use with minimal risk of vascular injury, and should not interfere with the actual TAVI procedure. The current devices are composed of a thin membrane with pores of about $100-200 \mu \mathrm{~m}$ size designed to allow normal blood flow but deflect or capture embolic material. While these devices certainly have the potential to reduce cerebral embolism, experience with TAVI is limited [57]. As TAVI is currently performed in elderly patients who often have very calcified arteries, it is possible that deployment of the protection device itself results in embolisation of some debris. In the future these devices may become more important if TAVI is performed in younger patients with a less calcified aortic arch where the main source of embolism is the valve itself.

## Vascular complications

## Clinical relevance of vascular complications

Despite the gradual decrease in sheath and catheter size, vascular complications remain one of the challenges in TAVI. Table 2 summarises the currently required sheath sizes for various valves. The Valve Academic Research Consortium (VARC) has proposed standardised definitions for clinical endpoints [60, 61]. Recently, VARC 2 has revised the VARC definitions and recommendations. According to the VARC, vascular complications include all complications that can be caused by a wire and/or are related to vascular access (e.g. major complications such as ventricular perforation, aortic dissection/rupture, iliofemoral rupture, iliofemoral dissection requiring treatment, and minor complications such as pseudoaneurysms or closure failure). Most of the recent publications reported the incidence of vascular complications according to these definitions, allowing direct comparison between studies. In such studies, major vascular complications have been reported in 5.6 to $17.3 \%$ [1, 4, 23, 41, 62-64]. In earlier studies, where

| Table 1: Predictors of cerebrovascular embolism/accidents after TAVI. |  |  |
| :--- | :--- | :--- |
| First author | Modality | Predictors of cerebrovascular embolism/accidents |
| Kahlert [45] | MRT | Renal dysfunction, lower aortic atheroma thickness, porcelain aorta. |
| Fairbairn [49] | MRT | Age, severity of aortic arch atheroma. |
| Szeto [54] | TCD | Severe calcification of aortic arch. |
| Miller [32] | Clinical | Cerebrovascular disease, smaller indexed aortic valve area, higher NYHA class, prior stroke, history of PCI, <br> COPD (lower risk). |
| Nuis [37] | Clinical | New onset atrial fibrillation, baseline aortic regurgitation $\geq 3$. |
| Rodes-Cabau [46] | Clinical | New onset atrial fibrillation. |

various definitions were used, vascular complication rates ranged from 1.9 to $11.7 \%$ [22, 44, 65-67].
Vascular complications have been associated with mortality, morbidity, reduced quality of life, and costs. 30 day mortality was found to be consistently higher in patients with vascular complications than those without (odds ratios ranging from 2.4 to 8.5 ) [42, 43, 62, 64, 68]. Pooled togeth-


Figure 5
Impact of vascular complications on 30-day mortality. 30-day mortality in patients with a (major) vascular complication was consistently higher than in those without. In pooled analysis of all 5 studies including $>1000$ patients, mortality was $16.9 \%$ (red dotted line) and 6.6\% (blue dotted line) in patients with and without vascular complications.


Figure 6
Screening of the iliofemoral arteries by fluoroscopy (A) and CT angiography (B).


Figure 7
Treatment of femoral artery injury by a covered stent. This patient presented with acute haemorrhage of the femoral artery (A). Bleeding was controlled by balloon tamponade, after which a Fluency Plus $9 \times 60 \mathrm{~mm}$ covered self-expanding stentgraft (Bard Canada Inc., Oakville, Canada) was implanted with a good result ( $B, C$ ).
er, all 5 studies included $>1,000$ patients. 30-day mortality in patients with vascular access complications was $16.9 \%$, in those without $6.6 \%$ (odds ratio $2.88,95 \%$ confidence interval 1.71-4.86, fig. 5 ). Furthermore, length of hospital stay was $\sim 5-7$ days longer in patients with vascular complications than in those without [62, 64].
The following risk factors for vascular complications have been identified: external sheath diameter $>$ minimal artery diameter, moderate or severe femoral calcification, presence of peripheral vascular disease, and centre experience (table 3) [62, 64, 67]. A smaller minimal iliofemoral diameter may be acceptable in the absence of circumferential or horseshoe shaped calcification, as the ability of the artery to expand is preserved. The presence of extensive tortuosity and aneurysms has not been associated with higher complication rates. The most important step to reduce vascular complication rates is therefore systematic access screening.

## Access screening and current sheaths

Screening of iliofemoral access is usually accomplished using fluoroscopic angiography and/or CT angiography (fig. 6 ). Several protocols have been developed to reduce the amount of contrast dye required for CT scans in patients with reduced renal function [69, 70]. Current sheaths used for TAVI are $30-35 \mathrm{~cm}$ long, have an inner diameter of 14-20 French and an outer diameter of $5.9-7.8 \mathrm{~mm}$. However, there are some exceptions. Following the slogan "think big", the larger $22-24 \mathrm{~F}$ sheaths are still required for TAVI in the USA. There are several expandable sheaths which are introduced in a low profile configuration reducing the risk of iliofemoral injury. The Edwards expandable introducer sheath (Edwards Lifesciences, Irvine, CA) has a compliant seam that allows transient expansion as the delivery catheter is passed through it [71]. After passage of the prosthesis the sheath contracts to some degree towards its unexpanded size. The SoloPath sheath (Onset Medical Corporation, Irvine, CA) is a balloon expandable sheath that is inserted in its unexpanded state with an outer diameter of only 4.3 mm , facilitating delivery through difficult anatomy. A balloon is then inflated to expand the sheath and reach the intended internal diameter of 18-21 F.

## Iliofemoral complications

Most centres have initially used a planned surgical cutdown to expose the iliofemoral artery to expose and control the artery above and below the puncture site $[1,4,21,44$, 68, 72, 73]. More recently the preclosure technique has been used employing ProStar or ProGlide devices (Abbott Vascular Inc, Redwood City, CA) [22, 26, 40, 41, 62-67, 74-76]. This facilitates performance of the procedure under conscious sedation with local anaesthesia, and allows earlier patient ambulation [77, 78]. However, a surgical cutdown might be particularly desirable in patients where a high puncture is needed due to extensive calcification, to a high femoral bifurcation, obesity, or the presence of a femoral stent/graft.
Iliofemoral complications are the most frequent vascular complications in transfemoral TAVI. On average, dissection of the iliofemoral arteries has been reported in $6.5 \%$ (range: 1.6-21.5\%), and iliofemoral rupture in 3.4\% (range
$0.7-9.3 \%)$ [21, 24, 44, 62, 64, 68, 74, 76, 70-81]. Mortality was $5.6 \%$ after iliofemoral dissection, but $30 \%$ after iliofemoral rupture. Other iliofemoral complications include bleeding ( $\sim 7.3 \%$ ), percutaneous closure failure ( $\sim 6.8 \%$ ), access site infection ( $\sim 2.3 \%$, chiefly after a planned surgical cut-down), pseudoaneurysms requiring intervention ( $\sim 1.5 \%$ ), and sheath avulsion (rare) [1, 4, $21-23,26,39-41,44,62-68,72-76,82]$.
Treatment of iliofemoral dissections depends on the extent and haemodynamic relevance. Usually, prolonged inflation of a balloon with appropriate diameter results in successful apposition of the intima and underlying media. More extensive dissection may warrant self-expanding or balloonexpandable stent deployment [83].
Similarly, treatment of iliofemoral rupture depends on the size of the rupture and the severity of bleeding. A smaller rupture may be difficult to diagnose since symptoms tend to be delayed and nonspecific (haemodynamic instability, groin/flank/abdominal/back pain). A computed tomography of the abdomen and pelvis allows rapid diagnosis. If the perforation is smaller, cross-over balloon inflation for up to 5-10 minutes may be enough to stop the bleeding. If there is ongoing bleeding, implantation of a covered stent (fig. 7 ) is often technically successful with high patency rates at mid-term follow-up [84]. Alternatively, surgical repair should be considered. In the presence of major injury, aortic balloon tamponade with an occlusion balloon may be life-saving.
Failed percutaneous closure may be treated with prolonged manual compression alone, or, in the case of ongoing or more severe bleeding, with balloon angioplasty, stent implantation or surgery. Pseudoaneurysms close spontaneously in $>50 \%$ of cases and can therefore be observed if the size is $<3-3.5 \mathrm{~cm}$, in the absence of pain, and if oral anticoagulation is not needed [85-87]. The treatment of choice is ultrasound-guided thrombin injection, which has
a success rate of almost $100 \%$ and a complication rate of $<1 \%$ [88-94].

## Complications of the aorta and ventricles

These severe complications include aortic dissection, rupture and left-right ventricular perforation, and are reported in $<2 \%$ of transfemoral TAVI but usually associated with a $>50 \%$ mortality rate $[64,74,76,81]$. Annular rupture may occur after balloon valvuloplasty or after implantation of an oversized valve. The risk of perforation may be higher with a balloon expandable valve and in patients with a very bulky, calcified valve which can perforate the sinus during valve implantation. Left ventricular perforation is usually caused by perforation with the stiff guidewire, by the crossing catheter (usually AL-1), or by the device nosecone. Right ventricular perforation is usually due to perforation with the temporary pacemaker wire. Annular or ventricular perforation often leads to pericardial tamponade, which causes hypotension and can be rapidly detected by transoesophageal or transthoracic echocardiography. If tamponade occurs, pericardiocentesis should be performed immediately. If haemostasis is unlikely, rapid surgical exploration and suture of the injury is usually technically successful. However, even with immediate treatment tamponade is often associated with (intraprocedural) death [79, 95].

## Need for a permanent pacemaker

Post-procedural conduction disorders requiring implantation of a permanent pacemaker (PPM) are more frequent after TAVI than after surgical AVR [96-98]. Mechanical trauma to the His bundle in the region of the subvalvular membranous septum, localised oedema and inflammation may contribute to atrioventicular conduction disorders fol-

| Valve | Commonly used sheaths (examples) | Sheath internal diameter | Sheath external diameter |
| :---: | :---: | :---: | :---: |
| Edwards Sapien 23 mm | RetroFlex 3 introducer sheath | 22 F | 8.4 mm |
| Edwards Sapien 26 mm | RetroFlex 3 introducer sheath | 24 F | 9.2 mm |
| Edwards Sapien XT 23 mm | NovaFlex introducer sheath | 18 F | 7.2 mm* |
|  | Edwards expandable sheath | 16 F | 6.6 mm* |
| Edwards Sapien XT 26 mm | NovaFlex introducer sheath | 19 F | 7.5 mm |
|  | Edwards expandable sheath | 18 F | 7.2 mm* |
| Edwards S3 26 mm | Edwards expandable sheath | 14F | 5.9 mm* |
| Edwards Sapien XT 29 mm | Edwards expandable sheath | 20 F | 7.8 mm* |
| Medtronic CoreValve 26-29 mm and St. Jude Portico 26 mm | St. Jude Medical Ultimum | 18 F | 6.8 mm |
|  | Cook Check-Flo Introducer | 18 F | 7.2 mm |
|  | Onset Medical SoloPath Balloon Expandable Transfemoral Introducer | 19 F | $7.3 \mathrm{~mm} \dagger$ |
|  | Gore Medical DrySheath | 18 F | 6.8 mm |

[^0] for the SoloPath Balloon Expandable Transfemoral Introducer. The unexpanded outer diameter is 4.3 mm .

| Table 3: Predictors of vascular complications. |  |  |
| :--- | :--- | :--- |
| First author | N | Predictors |
| Lange [67] | 412 | Centre experience, planned surgical cut-down reduced vascular complication rate. |
| Hayashida [64] | 130 | Sheath to femoral artery ratio (SFAR), femoral calcification, centre experience. |
| Toggweiler [62] | 137 | Sheath diameter > minimal artery diameter, moderate/severe femoral calcification, learning curve. |

lowing TAVI. Trauma may occur either directly by the implanted transcatheter heart valve or by compression through the calcified native aortic valve cusps. The most frequent disorder is a new left bundle branch block. Conduction disorders such as complete atrioventricular block or symptomatic bradycardia may occur acutely or delayed (more often with the Medtronic CoreValve), chiefly within the first week [96, 99].

## Frequency of pacemaker implant

Need for a permanent pacemaker has been reported in $\sim 6 \%$ (range: 3.4-22\%) of patients undergoing TAVI with the Edwards Sapien valve and $\sim 21 \%$ (Range: 16.6-42.5\%) with the Medtronic CoreValve [1, 4, 21, 23, 40, 43, 44, 63, 73, 79, 97]. In centres using both the Edwards Sapien and the CoreValve, a pre-existing RBBB may be a reason for using the Edwards Sapien valve to decrease the need for a PPM, but a recent study has shown that lower PPM rates can be achieved with higher implantation of the CoreValve [100]. In this study the targeted implantation depth of $4-6 \mathrm{~mm}$ was achieved in $69 \%$. A transient or sustained complete atrioventricular block occurred in $12.7 \%$, a pacemaker was implanted in $10.6 \%$ after a mean of $4.4 \pm 5.9$ days post TAVI. Another study reported a PPM rate of $11.7 \%$ after CoreValve implantation without balloon predilatation [101]. Using smaller balloons for valvuloplasty may also reduce the need for PPM.

## Predictors of pacemaker requirement

In a meta-analysis including a total of 5,258 patients a preexisting right bundle branch block (RBBB) and implantation of a CoreValve were the only predictors of pacemaker requirement [102]. Other studies have identified low implantation depth (of both Edwards Sapien and Medtronic CoreValve), valve oversizing, bradycardia, a pre-existing atrioventricular block, and higher age as risk factors for a new PPM [97, 98, 103-105]. In patients at high risk of PPM, prophylactic implantation of a PPM may be performed.

## Relevance of pacemaker implantation

Compared to other complications such as stroke, major vascular injury, death and acute severe paravalvular regurgitation, PPM implantation is considered a benign event. However, it does require an additional procedure, adds costs and may result in prolonged hospitalisation. Chronic right ventricular pacing may result in left ventricular dyssynchrony and reduced left ventricular contractility [106]. Survival up to 1 year follow-up was not worse in patients requiring a PPM after TAVI, but the long-term effects of right ventricular pacing are unknown [107].

## Conclusion

The safety and efficacy of TAVI have improved with nextgeneration low-profile equipment, experience and careful patient selection. Computed tomography allows more accurate annular and iliofemoral measurements, improving both valve sizing and selection of an optimal access route. Some of the next generation valves will allow repositioning and are designed to reduce paravalvular leaks. Hopefully
stroke rates will decrease with experience, optimal antithrombotic treatment and patient selection.

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Correspondence: Stefan Toggweiler, MD, Luzerner Kantonsspital, Spitalstrasse, CH-6000 Luzern 16, Switzerland, stefan.toggweiler[at]luks.ch

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Figures (large format)


Figure 1
Annulus sizing using TEE and CT angiography. TEE measured an annulus of 2.1 cm suggesting a 23 mm Edwards Sapien or a 26 mm Medtronic CoreValve (A). CT angiography measured an area of 481 mm 2 (C) and a mean diameter of 24 mm (B) suggesting a 26 mm Edwards Sapien or a 29 mm Medtronic CoreValve valve with $\sim 10 \%$ oversizing. A 26 mm Edwards Sapien valve was implanted with trace paravalvular leak (D).


Figure 2
Treatment of paravalvular regurgitation by implantation of a second transcatheter heart valve. In patient, the TEE measured an annulus of 22 mm . A 26 mm Edwards Sapien XT valve was implanted (A). A low implantation resulted in severe paravalvular aortic regurgitation (B, C). A second 26 mm valve was subsequently implanted in a higher position, thus extending the annular seal (D) resulting in a mild paravalvular leak (E, F).


Figure 3
Silent bilateral cerebrovascular emboli after transcatheter aortic valve implantation. Such diffuse, bihemispheric ischaemic lesions can be detected by MRT in 68-77\% of patients after TAVI.


Figure 4
Example of an embolic protection device. The Embrella embolic deflector (A, Embrella Cardiovascular Inc, Wayne, PA) is introduced through the right radial artery to protect the brachiocephalic artery (BA), the left carotid artery (LCA) and the left subclavian artery (LSA) during the procedure.


## Figure 5

Impact of vascular complications on 30-day mortality. 30-day mortality in patients with a (major) vascular complication was consistently higher than in those without. In pooled analysis of all 5 studies including >1000 patients, mortality was $16.9 \%$ (red dotted line) and $6.6 \%$ (blue dotted line) in patients with and without vascular complications.


Figure 6
Screening of the iliofemoral arteries by fluoroscopy (A) and CT angiography (B).


Figure 7
Treatment of femoral artery injury by a covered stent. This patient presented with acute haemorrhage of the femoral artery (A). Bleeding was controlled by balloon tamponade, after which a Fluency Plus $9 \times 60 \mathrm{~mm}$ covered self-expanding stentgraft (Bard Canada Inc., Oakville, Canada) was implanted with a good result (B, C).


[^0]:    * The pre-expanded diameter is indicated. The fully expanded diameter depends on the size of the catheter used for the procedure. $\dagger$ The final outer diameter is indicated

